

Capture and Analysis of Radiation Metrics From Fluoroscopic Procedures

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Improving radiation safety during fluoroscopic procedures requires a systematic approach where radiation metrics are routinely captured and analyzed and the results are used to determine if prior changes have led to improvement [1]. In this feedback loop, data is continually captured and analyzed.

Analysis uses a difference engine to calculate the difference between observed and predicted values of the various metrics. Substantial as well as systematic differences warrant an investigation to determine <u>causal factors</u> which might explain the difference [2]. The results are used not only to update the predicted values but also to suggest interventions that might lead to improvement. Repeating these cycles is the basis of continuous process improvement [3].

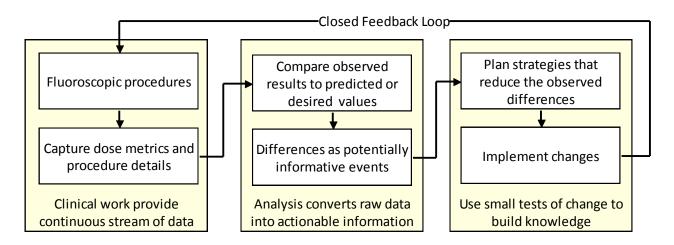


Figure 1: Continuous process improvement cycle

Like the underlying patient care systems, the resulting improvement system has internal processes that will evolve over time. The design of every component in this system aims to reduce the overall risks of these procedures while preserving their benefits.

Step 1: Capturing radiation metrics from every procedure

Several recent changes support the efficient and accurate capture of radiation metrics from fluoroscopic procedures. Newer fluoroscopy units record numerous dose metrics and record the values in a computer readable file [4]. These radiation dose structured reports (RDSRs) not only include the procedure's total fluoroscopy time, kerma area product and reference point air kerma, but also include underlying factors such as imaging protocol, tube current, kVP, pulse duration, frame rate, field of view, imaging angles, table position and detector position. Commercially available dose monitoring systems collect these reports and store the data in databases.

Despite these advances, neither the RDSRs nor the dose monitoring systems routinely collect all the data needed to fully describe the factors that influence a procedure's radiation use. Details of the procedure type, team performing the procedure, patient attributes and clinical history are not incorporated into the RDSR but could potentially be imported from other portions of the patient's electronic medical record. Such information could include the procedure and diagnostic codes (CPT[®], ICD-9 and ICD-10) used for billing purposes. Patient attributes such as size and anatomic factors could be extracted from the images themselves or an appropriately structured procedure report.

Step 2: Analyzing the data by finding large differences between observed and expected/desired

Data analysis can be viewed as the process of converting raw data into actionable information. One particularly effective analytic technique is to look for differences between observed and predicted values for various dose metrics.

Since <u>numerous factors</u> including patient size, operator skill, imaging protocols and difficulty of the clinical problem impact radiation use, predicted values are typically expressed as a range. Stated another way, it is fully expected that an intricate neurovascular intervention, difficult biliary drainage or complex percutaneous coronary intervention may require 10–30 minutes of fluoroscopy and results in $K_{a,r}$ (reference point air kerma) of 1000–3000 mGy. Conversely, it is unexpected that a simple insertion of an inferior vena cava filter, diagnostic arteriogram or feeding tube placement requires 10–30 minutes of fluoroscopy and results in fluoroscopy and results in $K_{a,r}$ of 1000–3000 mGy.

The more variable the underlying process, the more decisions are required to complete the procedure [5]. Since information gleaned from the fluoroscopic images is used to guide intraprocedural decisions, complex and variable procedures will tend to yield a larger expected range of dose metrics. One can begin to narrow the expected range by specifying the procedure in greater detail. As an example, when

all other factors are held equal, bilateral percutaneous nephrostomy tube placements are expected to result in longer fluoroscopy times and higher K_{a,r} than unilateral procedures.

Calculating expected ranges of dose metrics for common exams: internal vs. external benchmarks

The Joint Commission will soon require every imaging facility to develop expected ranges for its common CT procedures. Sites must also have a process for investigating what factor may have led to an exam falling outside that expected range.

While fluoroscopic procedures are far more variable than CT studies, the same processes should be used to develop expected ranges and investigate cases that fall outside the expected range. A site's prior results can be used to calculate the upper limit of the expected ranges for common fluoroscopic procedures.

While most sites will employ the 75th percentile used for calculating reference values, sites might also use <u>tools from statistical process control to calculate upper control limits</u>. Sites might also compare their results to external benchmarks such as those published by NCRP[6] or cited below [7,8].

Step 3: Planning improvement efforts and conducting small tests of change

Common explanations for large or systematic differences include imaging protocols, patient populations, procedure naming conventions or team skill. Single cases can be viewed as case-based learning opportunities. Case series with consistently higher than predicted/desired dose metrics warrant investigation for underlying factors such as imaging protocols or equipment calibration that warrant adjustment.

In the same way that CT protocols are being scrutinized for improvement opportunities, examination of fluoroscopy protocols can lead to changes in baseline settings and large and sustained reductions in $K_{a,r}$ across a wide variety of procedures [9].

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